

Original paper

The role of diffusion and perfusion magnetic resonance imaging in differentiation of haemangioblastomas and pilocytic astrocytomas

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Abstract

Purpose: Haemangioblastomas (HABLs) and pilocytic astrocytomas (PAs) are brain tumours presenting similar appearance and location in conventional magnetic resonance (MR) imaging. The purpose of our study was to determine whether a detailed analysis of diffusion (DWI) and perfusion (PWI) characteristics can be useful in preoperative differentiation of these tumours.

Material and methods: The study group consisted of biopsy proven six HABLs and six PAs, which underwent preoperative standard MR examinations including PWI and DWI. In PWI relative cerebral blood volume (rCBV) and the shape of perfusion curves (parameters of peak height – rPH and percentage of signal recovery – rPSR) were analysed. All perfusion parameters were measured for the entire tumour core (mean rCBV, mean rPH, mean rPSR) and in regions with maximal values (max rCBV, max rPH, max rPSR). In DWI parameters of apparent diffusion coefficient (ADC) from the entire tumour core (mean ADC) and in regions with minimal values (min ADC) were evaluated.

Results: Compared to PAs, HABLs presented significantly higher rCBV and rPH values and lower mean rPSR value. PAs showed significantly lower rCBV and rPH values and higher mean rPSR value. Mean rCBV showed no overlap in the values between HABLs and PAs, and thus it provided the highest accuracy in differentiating between them. Max rPSR, mean ADC, and min ADC did not show any significant differences.

Conclusions: High rCBV values and deep perfusion curves with only partial return to the baseline are characteristic features of HABLs differentiating them from PAs, which show lower rCBV values and perfusion curves overshooting the baseline. Diffusion parameters are not useful in differentiation of these tumours.

Key words: PWI, DWI, haemangioblastoma, pilocytic astrocytoma.

Introduction

Cerebellar haemangioblastomas (HABLs) and pilocytic astrocytomas (PAs) are two types of brain tumours that show similar appearance in conventional magnetic resonance (MR) imaging, typically presenting as a cyst with an associated mural nodule. Both of them are usually clinically benign and are classified as grade I by the World Health Organisation (WHO). The patient's age is often helpful in distinguishing these tumours associating HABLs with adult

patients and PAs with the paediatric population, but it is not always reliable [1,2]. Nevertheless, there is a group of young adults in whom both types of tumours may occur. Haemangioblastomas account for 1-2.5% of intracranial tumours and 7-12% of posterior fossa neoplasms in adult patients [3,4]. Pilocytic astrocytomas are the most common paediatric central nervous system (CNS) gliomas and one of the most common paediatric cerebellar tumours representing 60% of all astrocytomas in children [2]. They may also occur in adults, reaching in this group 2.3-6% of all brain tumours [1].

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A Study design · B Data collection · C Statistical analysis · D Data interpretation · E Manuscript preparation · F Literature search · G Funds collection

Morphologically, both HABLs and PAs may show heterogeneous appearance; mainly cystic but also solid-cystic or solid lesions are observed [3,4].

Both tumours are potentially curable by surgical resection and are associated with longer survival [5]. However, their histopathological structure has an impact on different clinical and surgical approaches. Since HABLs represent capillary-rich neoplasms of the CNS with large networks of tightly packed blood vessels lined by endothelial cells on a background of abundant connective tissue [6], their surgical resection should encompass the whole tumour capsule, otherwise it could lead to high mortality and morbidity rates due to the complication of excessive bleeding [3,7]. Sometimes preoperative embolisation of the feeding arteries may reduce the tumour blood supply, which can decrease intraoperative haemorrhage [8]. On the other hand, PAs, as less vascularised tumours, are composed of a variable combination of loose connective glial tissue, compacted piloid tissue, numerous vacuoles, microcysts, and sometimes macrocysts [6], so their potential complete resection is easier and safer.

As presented above, the reliable preoperative differentiation between HABLs and PAs is important but, in many cases, challenging in the standard MR imaging.

Advanced MR techniques such as perfusion-weighted imaging (PWI) and diffusion-weighted imaging (DWI) may add functional information and help in the *in vivo* characterisation of these two tumour types.

Perfusion-weighted imaging is the method that brings information on cerebral physiology at the capillary level (microvasculature) [9,10]. Among the PWI techniques dynamic susceptibility contrast (DSC) MR imaging is the most often used. DSC MRI provides maps of cerebral blood volume (CBV) and noninvasive measurements of relative cerebral blood volume (rCBV) [9,10] as well as perfusion curves, which give an insight into the dynamics of the first pass of the contrast material through the microvasculature. Analysis of perfusion curves has been reported to be very useful in the evaluation of brain tumours [9,10], in some cases more important than analysis of the CBV maps [10]. Two haemodynamic parameters derived from perfusion curves: the peak height (PH) and the percentage of signal intensity recovery (PSR), have been shown to provide important, additional information regarding tumor capillary volume and capillary permeability respectively [10].

On the other hand, DWI is a sensitive tool that allows quantifying of physiological alterations in water diffusion, which result from microscopic structural changes not detectable with anatomical MR imaging. Water diffusion can be measured with a parameter of apparent diffusion coefficient (ADC) [11,12]. Diffusivity of water depends primarily on the presence of microscopic structural barriers in tissue such as membranes of cell bodies, axons, and myelin sheaths but also viscosity of adjacent structures that can alter the random motion of water molecules. Highly cellular tumours show areas of restricted diffusion with

low ADC values, thus ADC is regarded as a marker of tumour cellularity [11,12].

In the literature there are a few reports that compare HABLs and PAs in advanced MR techniques, but none of them focuses on both DWI and PWI together in one study. The purpose of our study was to determine whether a detailed analysis of diffusion and perfusion characteristics with the evaluation of perfusion curves is useful in preoperative differentiation of these tumours.

Material and methods

The study group consisted of 12 solitary brain tumours, which were selected from a cohort of 1210 subjects with CNS tumours evaluated with T2**DSC* perfusion and diffusion MR in our institution between January 2010 and July 2017. Our material was subdivided into biopsy proven six HABLs (three men, three women) aged 32-73 years (mean age: 52 years) and six PAs (one man, five women) aged 14-67 years (mean age: 36 years). All tumours were solitary lesions located either infra- or supratentorially (Table 1).

Data acquisition

All examinations were performed on 1.5 T MR scanner (Signa Hdx, GE Medical Systems) using a 16-channel HNS (head-neck-spine) coil.

Before contrast administration a standard MR examination was carried out including axial T1-weighted images, axial, coronal, and sagittal T2-weighted images as well as axial FLAIR images followed by DWI and post-contrast DSC T2*-perfusion and 3D T1-weighted imaging.

During the whole MR examination the patients were instructed to keep their eyes closed. No sedation or anaesthesia were used in any of the patients.

Perfusion examination was performed with a dynamic susceptibility contrast (DSC) method using fast echoplanar T2*-weighted gradient echo sequence with the following parameters: TR = 1.900 ms, TE = 80 ms, FOV = 30 cm, matrix = 192 × 128, slice thickness = 8 mm without spacing, NEX = 1.0. Ten seconds after the start of the image acquisition a bolus of 1.0 mol/l gadobutrol formula (Gadovist, Bayer Health Care, Germany) in a dose of 0.1 ml/kg of body weight was injected via a 20-gauge catheter placed in the antecubital vein. Contrast was administered with an automatic injector (Medrad) at a rate of 5 ml/s and was followed by a saline bolus (20 ml at 5 ml/s). The whole perfusion imaging lasted 1 min 26 s, in which sets of images from 13 axial slices were obtained before, during and after contrast injection. After PWI a post-contrast T1-weighted 3D sequence was performed using contrast bolus administered earlier for the perfusion examination. No contrast agent was administered before DSC perfusion MR imaging.

Diffusion imaging was performed using a transverse single-shot echoplanar diffusion-weighted sequence with

Table 1. Demographic and imaging characteristics of haemangioblastomas and pilocytic astrocytomas

Patient	Age (years)	Sex	Location	Morphology	Enhancement
Haemangioblastomas					
1	73	Female	Cerebellum	Cystic with mural nodule	Homogenous
2	49	Female	Cerebellum	Solid	Homogenous
3	37	Male	Cerebellum	Cystic with mural nodule	Homogenous
4	63	Male	Cerebellum	Solid with necrosis	Inhomogenous
5	57	Female	Suprasellar region	Solid	Homogenous
6	32	Male	Peripheral, in the right temporal lobe	Solid with necrosis	Inhomogenous-peripheral
Pilocytic astrocytomas					
1	14	Female	Cerebellum	Cystic-solid with necrosis	Inhomogenous
2	63	Female	Cerebellum	Solid	Homogenous-peripheral
3	25	Female	Cerebellum	Solid	Inhomogenous
4	23	Female	Pperipheral, in the right frontal lobe	Solid	Homogenous
5	67	Male	Peripheral, in the left parietal lobe	Solid with necrosis	Inhomogenous-peripheral
6	26	Female	Suprasellar region	Solid with necrosis	Inhomogenous

the following parameters: TE = 89.9 ms, TR = 8000 ms, slice thickness = 5 mm, FOV = 26 cm, matrix size = 128 × 128, NEX = 1, diffusion sensitive gradient b = 1000 s/mm² in three basic orthogonal directions, scanning time: 42 seconds.

Data postprocessing

In all cases the morphological assessment of the lesions was performed on T1, T2-weighted, and post-contrast T1-weighted images using visual inspection.

The diffusion and perfusion weighted images were postprocessed using Functool software (ADW 4.4; GE Medical Systems).

Perfusion weighted imaging analysis

The analysis was based on evaluation of CBV parameters on CBV maps (Figure 1) as well as values of PH (peak height) and PSR (percentage of signal recovery) derived from perfusion curves. Measurements of CBV were per-

formed by placing ROIs on the CBV maps fused with post-contrast T1-weighted images to accurately assess the tumour core (Figure 1). PSR and PH were calculated from the perfusion curves based on the following formulas:

$$PSR = (S1 - Smin)/PH$$

$$PH = Smin - S0,$$

where: *S0* – start of contrast passage, *Smin* – maximal drop of magnetic susceptibility, and *S1* – measurement after 24 seconds from *Smin* (Figure 1). All CBV, PH, and PSR values were normalised to values from the normal appearing white matter of the contralateral hemisphere to obtain relative values of all parameters: rCBV, rPH, rPSR.

In each tumour measurements of mean values of all perfusion parameters for the whole tumour core (mean rCBV, mean rPH, mean rPSR) and maximal values of these parameters (max rCBV, max rPH, max rPSR) were assessed. Mean values for the whole tumour were obtained by manual outlining of the entire lesion on each slice (Figure 1) avoiding foci of haemorrhage or necrosis and calculating the arithmetical means from all the measured values. Maximal values were obtained by placing

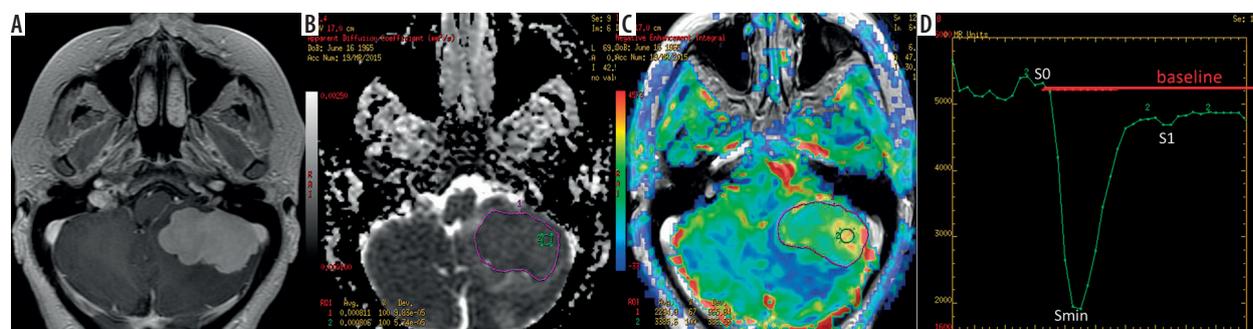


Figure 1. Haemangioblastoma in the left cerebellar hemisphere: (A) a post-contrast, T1-weighted image, (B) an ADC map, (C) a CBV map, (D) a perfusion signal intensity time curve. The ADC (B) and CBV (C) maps show placement of large irregular freehand ROIs outlining the tumour core (purple) as well as small circular ROIs within the big ROIs (green). The perfusion curve (D) shows haemodynamics of contrast agent during the first pass of a bolus through the brain vasculature, with the x-axis reflecting time in seconds and y-axis indicating signal intensity

small ROIs (40-60 mm²) within several hot spots on each slice. The highest value from all ROIs was chosen as the tumoural maximal value (Figure 1).

Diffusion-weighted imaging analysis

Measurements of ADC for the entire tumour (mean ADC) and measurements of minimum ADC (min ADC) were performed on ADC maps fused with post-contrast T1-weighted images. Similarly to perfusion evaluation, mean ADC values were obtained by manual outlining of the entire enhancing tumour core on each slice (Figure 1), avoiding foci of haemorrhage or necrosis, and then by calculating the arithmetical averages from all measured ADC values. Min ADC values were measured using small ROIs (40-60 mm²) located within the large freehand ROIs (Figure 1). The lowest value from all ROIs was chosen as the tumoural minimum ADC value described as min ADC.

Statistical analysis

All data obtained in the study were statistically analysed using the Statistica PL software package version 4.0. Quanti-

tative perfusion and diffusion data were compared between HABL and PA groups using the student *t*-test, with a *p* value below 0.05 set as the level of significance.

Results

Both HABLs and PAs were mainly located intra-axially in the cerebellum, although tumours in the supratentorial or extra-axial locations were also found (Table 1).

Based on standard MR examination HABLs and PAs presented variable morphology, both cystic and solid (Table 1, Figures 2 and 3). Compared to PAs, HABLs more often showed typical appearance of a cyst with a mural nodule as well as homogenous enhancement (Table 1, Figure 2). On the other hand, the majority of PAs were solid with areas of necrosis and inhomogeneous enhancement (Table 1, Figure 3).

All HABLs presented very high perfusion parameters of mean rCBV (6.44), max rCBV (12.01), mean rPH (5.31), max rPH (9.00) as well as low values of mean rPSR (0.21) and max rPSR (0.53), indicating only a slight return of the perfusion curve to the baseline level. Compared to HABLs, PAs showed significantly lower mean rCBV (2.14), max

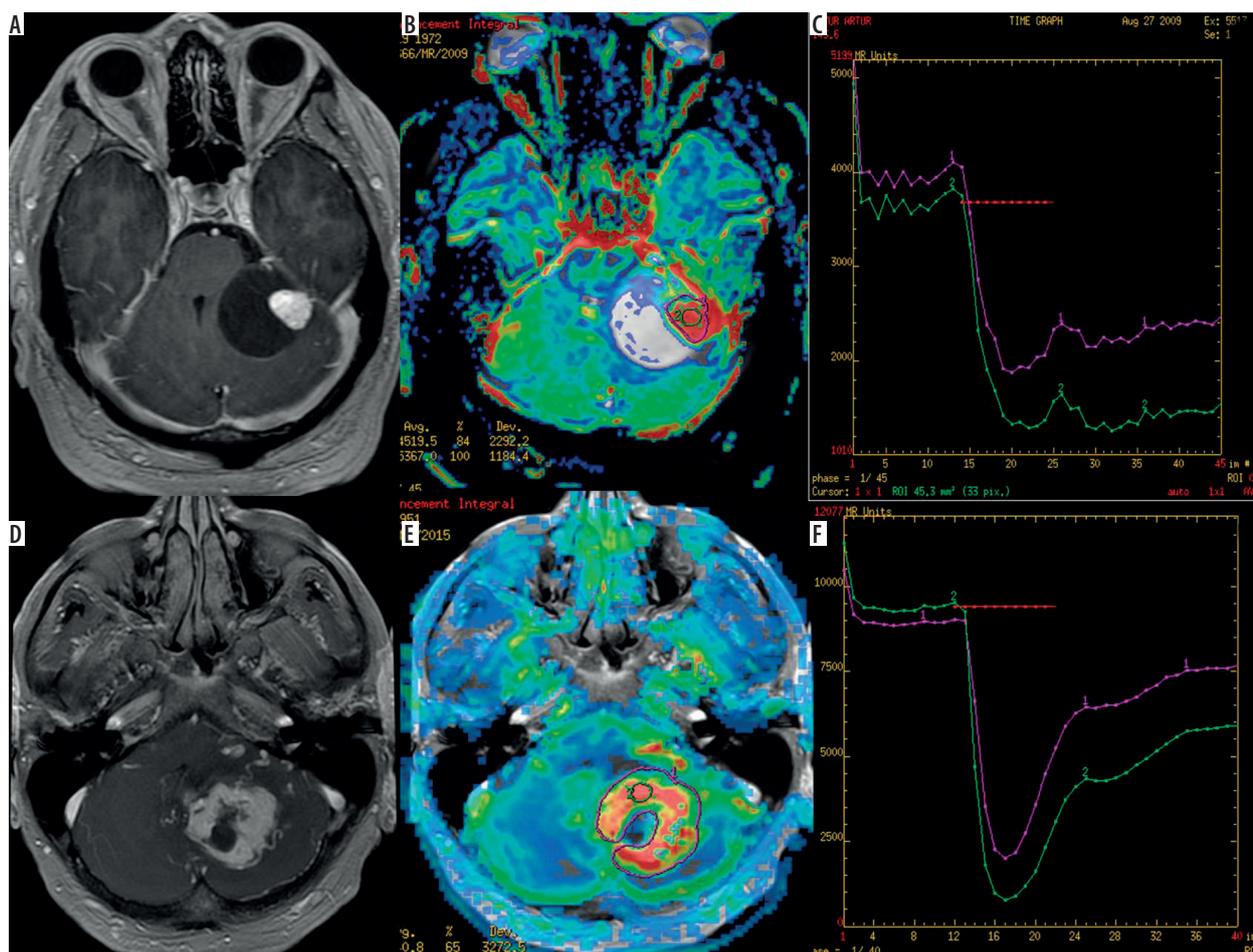


Figure 2. Two examples of haemangioblastomas in the cerebellum presenting as a cystic tumour with a mural nodule (A) and as a more solid tumour (D) on post-contrast T1-weighted images. CBV maps (B and E) show high perfusion values indicated by red colour while perfusion curves (C and F) present only partial return to the baseline level (red lines)

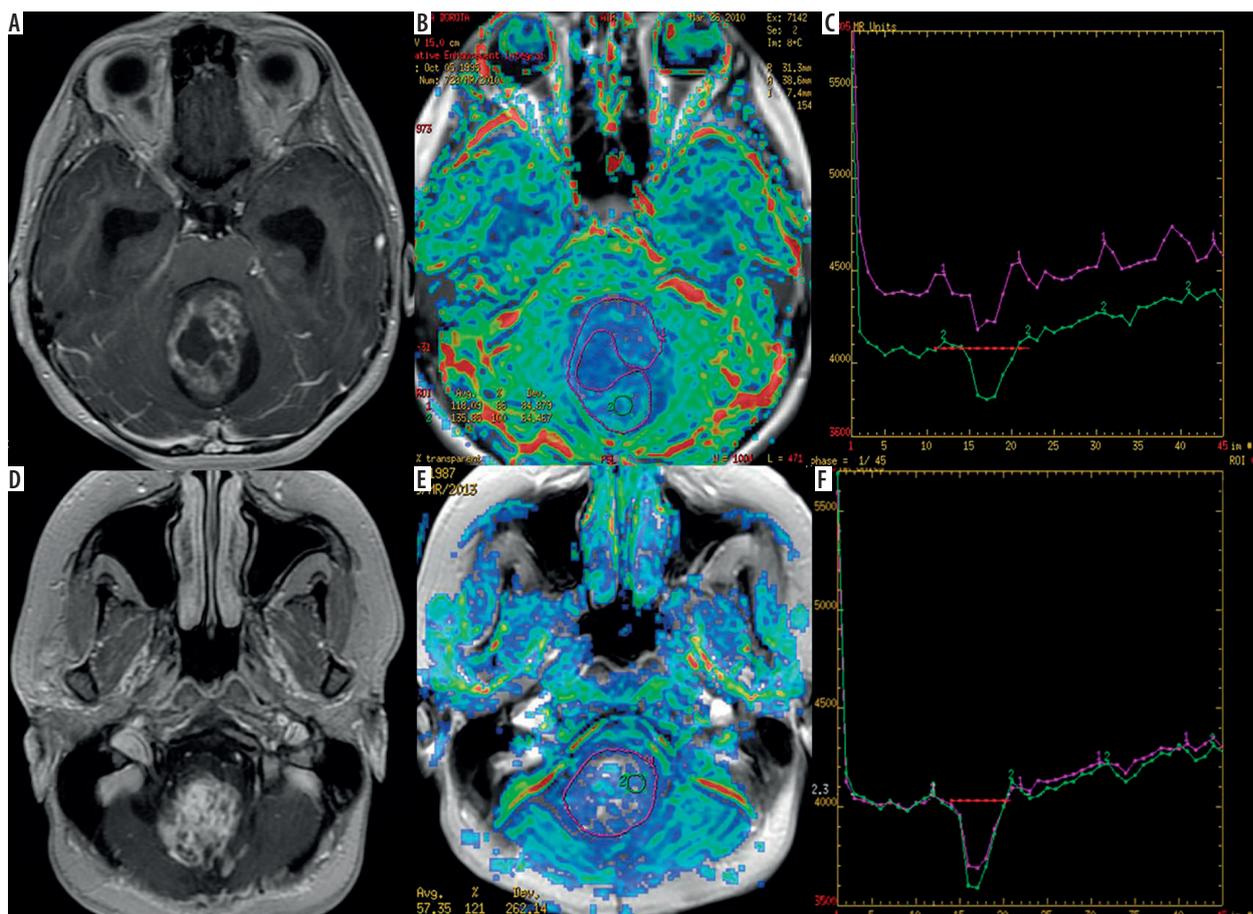


Figure 3. Two examples of pilocytic astrocytomas presenting as cystic-nodular (A) and solid tumours (D) on post-contrast T1-weighted images. CBV maps (B and E) show low perfusion values indicated by green and blue colours while perfusion curves (C and F) present return above the baseline level (red lines)

Table 2. Perfusion and diffusion measurements with the results of group comparisons indicated by *p*-value

Patient	mean rCBV	max rCBV	mean rPH	max rPH	mean rPSR	max rPSR	mean ADC	min ADC
Haemangioblastomas								
1	8.22	10.91	5.58	10.32	0.30	0.36	1.73	1.41
2	5.1	9.10	5.1	9.65	0.30	0.98	0.81	0.76
3	6.75	10.50	6.64	8.34	0.42	0.45	1.67	1.29
4	9.13	22.07	5.90	9.65	0.20	0.70	1.68	1.31
5	3.74	4.85	3.51	4.07	-0.40	0.10	1.88	1.63
6	5.71	14.61	5.13	11.99	0.46	0.56	1.11	0.69
Mean	6.44	12.01	5.31	9.00	0.21	0.53	1.48	1.18
Pilocytic astrocytomas								
1	1.34	2.64	3.65	4.84	5.04	5.84	1.14	0.84
2	2.67	3.54	2.51	3.21	0.97	1.00	0.84	0.65
3	2.93	9.62	2.72	8.05	0.43	1.07	1.62	1.06
4	1.27	1.82	2.11	2.38	1.83	1.84	1.05	0.94
5	3.34	6.34	1.94	3.51	1.10	1.12	1.00	0.70
6	1.30	1.81	1.82	2.07	1.71	1.74	1.05	0.82
Mean	2.14	4.30	2.46	4.01	1.85	2.10	1.11	0.84
<i>p</i> -value	0.0007*	0.01*	0.0002*	0.005*	0.03*	0.06	0.1	0.06

*Statistically significant values

rCBV (4.30), mean rPH (2.46), and max rPH (4.01) as well as significantly higher mean rPSR (1.85) and max rPSR (2.10) (Table 2). There were overlaps in parameters of max rCBV, mean rPH, max rPH, mean rPSR, and max rPSR but no overlap in the values of mean rCBV. Mean rCBV was found to be a parameter showing the highest accuracy in distinguishing these two analysed types of tumours (Table 2).

In DWI the values of mean ADC and min ADC were slightly higher in the HABL group (1.48 and 1.18, respectively) than in PAs (1.11 and 0.84, respectively). Moreover, there was an overlap in ADC values between HABLs and PAs (Table 2). No statistically significant differences were observed between average values of these parameters.

Discussion

Regarding the typical morphological appearance of both tumours as a cystic mass with enhancing mural nodule located in the cerebellum, our observations on conventional MR examination demonstrated many exceptions in both tumour location and morphology. In our study only one third of HABLs showed the typical morphological appearance as a cystic mass with a mural nodule located in the cerebellum (Table 1, Figure 2). Brundl *et al.* [3] analysed the morphology of 12 HABLs, reporting eight of them to have a typical appearance, which was 66.7% of the study group, whereas Kumar *et al.* [6] presented 50% of HABL tumours as typically appearing. Analysing PA cases, half of them were located extracerebellarly. The majority of PAs appeared solid and inhomogenous and only one case presented typically as a cystic mass with an enhancing nodule in the cerebellum (comprising only ~16.7% of our PA cases) (Table 1, Figure 3). A study by Burkhard *et al.* [2] also analysed the location of PAs and showed that minority of cases (around 42%) were located typically in the cerebellum. Moreover, Burkhard *et al.* [2] observed the tendency of PAs in children under 12 years old to be located typically in the cerebellum, contrary to adult patients. On the other hand, Stüer *et al.* [1] reported that only 21% of PAs presented a typical morphological appearance as a cystic mass with a mural nodule.

The variations and similarities in the presentation of HABLs and PAs reported in the literature [1-3,6,8] coincide with our results and experience. It proves the importance of advanced MR techniques such as PWI and DWI, which can provide additional information on a microstructural level, which may in turn help in the differentiation between both tumour types in terms of their vascularisation and cellularity.

In our study we used PWI to evaluate tumour vascularisation and DWI to assess cellularity. Analysing perfusion studies we found significant differences between HABLs and PAs regarding both rCBV values derived from rCBV maps as well as shapes of perfusion curves.

Compared to PAs, HABLs showed significantly higher values of mean CBV and max CBV (Table 2, Figures 2 and 3),

reflecting their high vascularisation. The parameter of rCBV was also evaluated by several other authors, and our results are in agreement with these studies [6,8,13].

It must be stressed that in our study mean rCBV was the only perfusion parameter without any overlap in the values between two tumour types, with a range of 1.27-3.34 in PAs and 3.74-9.13 in HABLs, and therefore mean rCBV may be regarded as the parameter with the highest accuracy in distinguishing between both tumours.

In our opinion, analysis of perfusion curves may also be useful in differentiation between HABLs and PAs because these two tumour types show different shapes of signal intensity time curves. Our study revealed that in HABLs the signal drop described as PH was more pronounced, in contrast to PAs where the signal drop was relatively small (Table 2, Figures 2 and 3). The differences in both mean rPH and max rPH were statistically significant with *p*-values 0.0002 and 0.005, respectively. Moreover, in HABLs signal recovery described as rPSR was less pronounced, with only partial return of the perfusion curve to the baseline level. In our study the majority of PA cases showed the signal time intensity curves crossing the baseline (overshooting) after the first pass; however, only mean rPSR values reached the level of significance.

Our results of the PH parameter are in agreement with the study by She *et al.* [14], who also showed statistically higher values of PH in HABLs than in PAs. On the other hand, the results of our PSR analysis only partially remain in agreement with the above mentioned study by She *et al.* [14], who found both max rPSR and mean rPSR to be higher in PA.

The differences in either rCBV or rPH values between HABLs and PAs may be explained easily by the distinct histological features of these two tumour types. As mentioned before, HABLs have abundant tumour vessels within lesions shown by high rCBV values and more pronounced signal drop reflected in rPH values, whereas PAs are sparsely vascularised in a wide interstitial space contributing to less pronounced perfusion curves and lower rCBV values [6,14].

The explanation of PSR characteristics in both tumours is complicated because it is influenced by many factors, including the permeability of capillaries, the amount of contrast agent leakage, the rate of blood flow, as well as the size of extravascular space [14,15]. Moreover, the signal intensity is connected with the complex T1- and T2*-shortening effect from the accumulation of contrast agent in the interstitial space of lesion. When the T1-shortening effects, due to accumulation of contrast agent in the interstitial space, overwhelm the T2*-shortening effects, the signal intensity increases and even exceeds the baseline level [14,15]. The significant difference in the mean rPSR between HABLs and PAs in this study may suggest that contrast agent leakage into the interstitial space in PAs is more pronounced than that in HABLs [8].

In our study DWI was proved to be a less specific and sensitive method in differentiation HABLs from PAs with

no statistical significance. However, HABLs presented higher values of both mean ADC as well as min ADC in comparison to PAs (Table 2). Higher ADC values may be explained by a lower rate of cellularity in HABLs compared to PAs, and it may suggest the diagnosis of HABL in the posterior cranial fossa [16]. On the other hand, the results of ADC values in HABLs as well as in PAs appear similar to other benign tumours, which is consistent with previous reports [8,17,18] and may help in differentiation from high grade tumours (Table 2).

Conclusions

Perfusion measurements are more useful than diffusion parameters in differentiation between HABLs and PAs.

High rCBV values and deep perfusion curves with only partial return to the baseline measured within the whole enhancing tumour part characterise HABLs and

enable differentiation of them from PAs showing lower rCBV values and the curve overshooting the baseline.

The mean rCBV value showed no overlap in the values between HABLs and PAs, and thus it provided the highest accuracy in distinguishing between these tumour types.

Perfusion MR, as an easy to perform and rapid technique, should be routinely used in differentiation of brain focal lesions, including distinguishing HABLs from PAs.

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Conflict of interest

The authors report no conflict of interest.

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